



THE UNIVERSITY *of* EDINBURGH

Edinburgh Research Explorer

## Variability of within-step acceleration and daily wellness monitoring in Collegiate American Football

**Citation for published version:**

Murray, A, Andrew, B, Alec, S, Sproule, J & Turner, A 2019, 'Variability of within-step acceleration and daily wellness monitoring in Collegiate American Football', *Journal of Science and Medicine in Sport*, vol. 22, no. 4, pp. 488-493. <https://doi.org/10.1016/j.jsams.2018.10.013>

**Digital Object Identifier (DOI):**

[10.1016/j.jsams.2018.10.013](https://doi.org/10.1016/j.jsams.2018.10.013)

**Link:**

[Link to publication record in Edinburgh Research Explorer](#)

**Document Version:**

Peer reviewed version

**Published In:**

Journal of Science and Medicine in Sport

**General rights**

Copyright for the publications made accessible via the Edinburgh Research Explorer is retained by the author(s) and / or other copyright owners and it is a condition of accessing these publications that users recognise and abide by the legal requirements associated with these rights.

**Take down policy**

The University of Edinburgh has made every reasonable effort to ensure that Edinburgh Research Explorer content complies with UK legislation. If you believe that the public display of this file breaches copyright please contact [openaccess@ed.ac.uk](mailto:openaccess@ed.ac.uk) providing details, and we will remove access to the work immediately and investigate your claim.



1 **Title:** Variability of within-step acceleration and daily wellness monitoring in Collegiate  
2 American Football

3 **Submission Type:** Original Investigation

4 **Authors:** Murray, Andrew<sup>1,2</sup>; Buttfield, Alec<sup>3</sup>; Simpkin, A<sup>4</sup>; Sproule, John<sup>1</sup>; Turner, Anthony P<sup>1</sup>

5 <sup>1</sup>Institute of Sport, PE & Health Sciences, University of Edinburgh, Edinburgh, UK

6 <sup>2</sup>University of Oregon, Athletics, 2727 Leo Harris Parkway, Eugene, Oregon, USA 97401

7 <sup>3</sup>Institute of Sport, Exercise and Active Living College of Sport and Exercise Science, Victoria  
8 University

9 <sup>4</sup>School of Mathematics, Statistics and Applied Mathematics, National University of Ireland,  
10 Galway, Ireland

11 **Contact details:**

12 Andrew Murray

13 University of Oregon

14 Athletics Department

15 2727 Leo Harris Parkway

16 Eugene

17 OR 97401

18 [amurray2@uoregon.edu](mailto:amurray2@uoregon.edu)

19

20 **Running Title:** Step Variability & Wellness in American Football

21 **Declarations of interest:** None

22 **Word Count:** 3496

23 **Abstract word Count:** 192

24 **Figures:** 1

25 **Tables:** 2

26

27 **Abstract**

28 **Objectives:** It is commonplace to consider accelerometer load and any resultant neuromuscular  
29 fatigue in training programs. With these data becoming accepted in sport alongside wellness  
30 questionnaires this study aimed to investigate if a deeper analysis of the accelerometry data can  
31 provide actionable insight into training-induced disruptions.

32  
33 **Design:** Accelerometer data from Collegiate American Football athletes (n=63) were collected  
34 during training and matches across a regular season.

35  
36 **Methods:** These data were processed to: identify instances of high speed running, extract step  
37 waveforms from those sections, and determine the variability of those waveforms via a within-  
38 and between-section co-efficient of multiple determination. Athletes completed wellness  
39 questionnaires prior to sessions that were used to flag areas of muscle soreness as well as fatigue,  
40 or disturbed sleep quality. Linear mixed models were used to assess associations between intra  
41 stride variability and flags in wellness/soreness markers.

42  
43 **Results:** An increase in acute (7d) load saw an increased stride variability in these athletes. Feeling  
44 less fatigued and/or lower muscle soreness was associated with higher stride variability.

45  
46 **Conclusion:** The assessment of variability has the potential to identify athletes who are displaying  
47 physical symptoms that would indicate the need to modify training.

**48 Introduction**

49 Movement variability exists even in highly trained skills performed by elite athletes,<sup>1</sup> this would  
50 suggest that gait would also reflect the theoretical principle of a ‘healthy’ amount of movement  
51 variability. Indeed, individuals with patellofemoral knee pain have been shown to exhibit reduced  
52 movement variability compared to a healthy group.<sup>2</sup> Although subsequent studies have produced  
53 contradictory findings,<sup>3</sup> movement variability has been shown to increase in subjects affected by  
54 patellofemoral pain when their pain is reduced through a therapeutic intervention<sup>3</sup>, suggesting  
55 there is an individual level of movement variability in gait and that variability is decreased when  
56 pain is present. Increased fatigue has been shown to lead to increased variability in knee  
57 kinematics during a cutting maneuver, which in turn will lead to a reduced ability to produce a  
58 controlled movement.<sup>4</sup> Consequently, the use of movement variability as a clinical tool to identify  
59 when an individual has a less than optimal movement pattern, is entirely possible as long as the  
60 chosen measurement tool has sufficient resolution to identify significant changes in an individual’s  
61 movement variability.

62  
63 Wireless accelerometry is a popular approach to continuously assess both proximal (e.g. trunk)  
64 and distal (e.g. tibial) mechanics in human locomotion unobtrusively. This approach is common  
65 in inertial measurement units that are used with athletes and are worn on the torso – typically  
66 incorporating accelerometers, global positioning systems (GPS), magnetometers, and gyroscopes.  
67 Using this approach the magnitude of peak accelerations have been validated<sup>5</sup> which demonstrates  
68 that filtered data collected by a MinimaxX S4 unit (Catapult Sports, Australia) provides an  
69 acceptable means of assessing peak accelerations (CV=8.9%). An alternate unit (SPI HPU,  
70 GPSports, Canberra, Australia) has been shown to accurately identify temporal stride  
71 characteristics (contact time  $r=0.98$ ; flight time  $r=0.68$ ) when compared to an instrumented  
72 treadmill<sup>6</sup>. Ankle movement was constrained through taping and two of the three variables  
73 examined (contact time and vertical stiffness) correctly identified side-to-side differences in stride

74 characteristics. These findings confirm the ability of this and similar units incorporating GPS and  
75 accelerometers, to identify small but practically important differences in stride characteristics due  
76 to physical constraints within a laboratory setting. This is particularly useful to applied  
77 practitioners given the practical and economic aspects of accelerometer technology.

78  
79 The coefficient of multiple determination (CMD) and related coefficient of multiple correlation  
80 (CMC) have previously been used to analyze many forms of cyclic kinematic and kinetic data that  
81 have ranged from an analysis of kinematic variability in gymnastics<sup>7</sup> to electromyographic,  
82 kinematic and kinetic measures of ice hockey skating<sup>8</sup>. Assessing the variability of waveforms has  
83 previously been done with gait data and been shown to be valid as a measure of stride  
84 characteristics via a single tri-axial accelerometer mounted on the upper torso<sup>9</sup>. Such analysis  
85 examines the waveform in its entirety rather than at specific points such as at foot strike or toe-  
86 off, and therefore accurate identification of specific points within the gait cycle will be less  
87 influential on the result of the analysis. In addition, using CMD to determine waveform variability  
88 does not require the waveforms to be from a continuous time period. This is a crucial consideration  
89 when analyzing data collected in gameplay and training rather than controlled laboratory settings.

90  
91 It is common place to take accelerometer and GPS-derived running loads into consideration for  
92 the management of athletes<sup>10,11</sup>. With these data becoming commonplace in the sporting world  
93 alongside wellness questionnaires<sup>12</sup> and athletes self-reporting muscle symptoms. This study  
94 aimed to investigate if a deeper analysis of the accelerometry data can be used to explore  
95 relationships between load, wellness, soreness and stride variability to provide actionable insight  
96 into training induced disruptions.

97

## 98 **Methods**

### 99 *Participants*

100 Data from 63 American Football athletes ( $20.6 \pm 1.5$  yrs;  $102.4 \pm 20.1$  kg;  $186 \pm 7.7$  cm) operating at  
101 the Division 1 level in the NCAA were collected across a regular season. Athletes provided  
102 informed consent to participate in data collection throughout the season as part of the athlete  
103 support process and the institutional ethics committee provided ethical approval for the research.

104

#### 105 *Design*

106 Inertial measurement units (IMU) containing GPS and accelerometers (Optimeye S5, Catapult  
107 Sports, Australia) were worn for every field session. The data collected and used in these studies  
108 were from the tri-axial accelerometer (measured at 100 Hz). For the purposes of this observational  
109 study, with repeated measures on the participants, only data from the main training sessions  
110 (Tuesday and Wednesday) and the match (Saturday) were recorded. This means light walk-  
111 through sessions on Sunday and Thursday were excluded, as were Friday sessions that were short  
112 and light in comparison to other sessions.

113

#### 114 *Methodology*

##### 115 *Accelerometry*

116 The 100Hz accelerometer data were processed with a novel analysis tool developed specifically  
117 for identifying instances of high speed running and determining the variability of the remaining  
118 waveforms via a within-section and between-section CMD. The raw files were exported via the  
119 manufacturer's software (Catapult Sports, Openfield software, version 1.11.1). A step frequency  
120 of 2.75 steps per second for at least five seconds was chosen as the lower limit for high speed  
121 running. This step frequency was chosen after pilot testing (with the aim of achieving a similar  
122 number of step waveforms available for further analysis as was achieved in previous applications  
123 of the analysis tool)<sup>9</sup> and is in general agreement with previous research.<sup>13</sup>

124

125 Accelerometer data from those sections of high speed running were analyzed to identify steps  
126 through identifying foot strike events via peaks in the vertical accelerometer data. The step  
127 waveforms likely to have been influenced by gameplay demands were identified as steps where  
128 the mean vertical acceleration in the first 20% of the step was at least 2 standard deviations greater  
129 or less than the mean vertical acceleration for the first 20% of all steps on that day – these were  
130 eliminated from the analysis. Step waveforms were separated into left and right-side steps by  
131 examining the lateral accelerations, with steps displaying a negative to positive acceleration  
132 around foot strike being designated right side steps and vice versa. The CMD was then calculated  
133 on the set of vertical (z-axis) step waveforms to determine the variability of those waveforms as  
134 per Kadaba and colleagues<sup>14</sup>. CMD values were calculated for each session for each player. They  
135 were combined over sections of high speed running during each game and CMD values were  
136 calculated from the within and between-stride variability, and then averaged over all sections of  
137 high speed running and turned into percentage of variation to improve interpretability. The data  
138 were therefore hierarchical in nature, with strides nested within sections within games within  
139 players. However, section-level data were unavailable for analysis.

140  
141 Different calculations of variability were performed, one to examine the waveform variability  
142 within each section of high speed running, another to examine the variability between sections of  
143 high speed running. In all calculations, higher CMD scores indicate less waveform variability. All  
144 calculations occurred on the vertical axis as it has been shown previously that this is the most  
145 sensitive as a load indicator<sup>9</sup>.

146

#### 147 *Wellness*

148 Over the course of the season the athletes completed a wellness questionnaire on training days, as  
149 used previously in the literature.<sup>12</sup> This recorded any areas of soreness as well as noting their  
150 fatigue, sleep quality and overall muscle soreness (1=poor, 5=good). As part of the wellness

151 questionnaire athletes noted any specific locations of soreness and then rated these in term of  
152 severity (1-10). Any area greater than a 5 out of 10 for pain triggered a ‘flag’ to the practitioners  
153 working with the athletes. These flags are considered compromised training days in this study.

154

#### 155 *Load*

156 IMU determined daily workloads (Playerload™) were calculated and expressed as arbitrary units  
157 (AU) via the manufacturer’s software (Catapult Sports, Openfield software, version 1.11.1) for  
158 every session. Participants wore the same device during every training session and match. Rolling  
159 loads for acute and chronic periods were calculated before sub setting the data to the main training  
160 sessions and games. The acute period was defined as 7 days and the chronic as 21 in line with  
161 previous American Football research.<sup>15</sup>

162

#### 163 **Statistical Analysis**

164 All analyses were carried out using R v3.5 (R Core Team (2018). R: A language and environment  
165 for statistical computing. R Foundation for Statistical Computing, Vienna, Austria URL  
166 <https://www.R-project.org>). Since repeated measures per player were available, linear mixed  
167 models were used to account separately for within-player and between-player variability in CMD  
168 values, while investigating their association with wellness (fatigue, sleep, soreness) and load  
169 (acute (7-day average), chronic (21-day average) and acute-chronic workload ratio) on that day.  
170 A random intercept term for player was used to allow for different average CMD values between  
171 athletes, while random slope terms allowed for different changes over time in CMD between  
172 players. A random effect for side of measurement was tested but led to convergence issues, hence  
173 it was included only as a fixed effect. To account for nonlinear changes in CMD over time,  
174 quadratic and cubic time terms were included as fixed and random effects. An AR1 process was  
175 included for within-subject variability to account for auto-regressive aspect of CMD during the



176 period of measurement. In each model, we also controlled for the number of strides, number of  
177 sections and side of measurement (left/right leg) to account for confounding. The association  
178 between each measure of wellness and load with CMD are presented as coefficients with 95%  
179 confidence intervals and p-values. Model residuals were checked to validate the assumptions  
180 underlying the linear mixed model. In order to compare between the load and wellness markers,  
181 we took the z-score of each of these (fatigue, sleep, soreness, ACWR, acute load, chronic load)  
182 and repeated analysis, with the resulting coefficients plotted showing the effect of a 1 standard  
183 deviation change in exposure. A secondary analysis focused on compromised training. Here a  
184 generalized linear mixed model was used to model flagged injury status against unflagged status  
185 for hamstring, ankle and foot injuries separately. The key variables under examination were within  
186 and between stride CMD measured during the flagged and unflagged strides. In each model, we  
187 included day of measurement as a fixed effect and used a random effect for athlete to allow each  
188 to have their own intercept. A logit link was used to model the three (hamstring, ankle and foot)  
189 binary outcomes (injured v not injured), and odds ratios are reported alongside 95% confidence  
190 intervals and p-values. Model residuals were again checked to validate the assumptions underlying  
191 the mixed model.

192

### 193 **Results**

194 Descriptive statistics for the key variables in the study are given in Table 1. All wellness variables  
195 had a mean of ~3, while acute (7-day) load was slightly higher than chronic (21-day) load. There  
196 were  $4.94 \pm 5.75$  ( $\pm$ SD) sections of high speed running per session across players on average, with  
197 a mean of  $47.65 \pm 69.68$  strides within a section. Figure 1 shows the nonlinear changes in CMD  
198 over the period of measurement, with similar patterns of change for within-stride and between-  
199 stride CMD.

200

\*\*\*TABLE 1 NEAR HERE\*\*\*

201

\*\*\*FIGURE 1 NEAR HERE\*\*\*

202

203 *Wellness*

204 There was some evidence for an inverse relationship between fatigue and between-stride CMD.

205 A one-point increase in fatigue score (i.e. feeling better) being related to a 0.508% decrease in

206 between-stride CMD (increased variability; table 2; 95% CI -0.953, -0.063%, p=0.025). There

207 was no evidence for a relationship between sleep score and either within- or between-stride CMD.

208 Finally, there was evidence for a negative association between soreness and CMD. A one-point

209 increase in soreness score (i.e. less sore) was related to a 0.337% decrease in mean within-stride

210 CMD (increased variability; table 2; 95% CI -0.670, -0.005%, p=0.047) and a 0.356% decrease in

211 mean between stride CMD (table 2; 95% CI -0.752, 0.039%, p=0.078).

212

213 **\*\*\*TABLE 2 NEAR HERE\*\*\***

214

215 ACWR had a negative effect on both within and between stride CMD, with a 1 unit increase in

216 ACWR associated with a 6.849% decrease in mean within-stride CMD (increased variability; 95%

217 CI -8.580, -5.117%, p&lt;0.001) and a 7.257% decrease in mean between stride CMD (increased

218 variability; 95% CI -9.355, -5.160%, p&lt;0.001). Acute load (7-day average) was also associated

219 with within- and between stride variability. A one unit increase in acute load was related to a

220 0.012% decrease in mean within-stride CMD (increased variability; 95% CI -0.016, -0.009%,

221 p&lt;0.001) and a 0.013% decrease in mean between stride CMD (increased variability; 95% CI -

222 0.017, -0.010%, p&lt;0.001). Finally, an increase in chronic load (21-day average) was also inversely

223 related to within- and between-stride CMD. A one unit increase in chronic was associated with a

224 0.007% decrease in mean within-stride CMD (increased variability; 95% CI -0.011, -0.002%,

225 p=0.002) and a 0.005% decrease in mean between stride CMD (increased variability; 95% CI -

226 0.011, 0.000%, p=0.034).

227

**\*\*\* FIGURE 2 NEAR HERE\*\*\***

228 *Comparing load and wellness*

229 In order to compare the standardized coefficients across load and wellness where each exposure  
230 variable has been z-scored with the resulting coefficients showing the effect of a 1 standard  
231 deviation change in exposure (Figure 2). In this plot, the coefficients can be better compared. From  
232 Figure 2, acute load appears to have the strongest effect on within-stride CMD (-1.400%, 95% CI  
233 -1.751, -1.048%;  $p < 0.001$ ), followed by ACWR (-1.055%, 95% CI -1.322, -0.788%;  $p < 0.001$ ) and  
234 chronic load (-0.659%, 95% CI -1.079, -0.239%;  $p = 0.002$ ), with wellness measures having a  
235 weaker (per-SD) effect on CMD. Similarly, for between-stride CMD, load had a stronger effect  
236 in the same order, with acute being strongest (-1.493%, 95% CI -1.914, -1.073%;  $p < 0.001$ )  
237 followed by ACWR (-1.118%, 95% CI -1.441, -0.795%;  $p < 0.001$ ) and chronic load (-0.532%,  
238 95% CI -1.022, -0.041%;  $p = 0.034$ ).

239

240 *Compromised training*

241 Table 3 summarizes the models of compromised training and the effect of within and between  
242 stride CMD on these episodes. There were 9, 22 and 26 flagged hamstring, ankle, and foot injuries  
243 respectively. There was no strong evidence for an association between within or between stride  
244 CMD on any of the injury sites. However, given the small number of episodes, this analysis is  
245 underpowered. Within the sample, a one unit increase in between stride CMD was related to 3  
246 times the odds of compromised training (odds ratio 3.111), but the interval estimate here is  
247 extremely wide (95% CI 0.297, 32.553) due to so few ( $n=9$ ) hamstring episodes.

248 **\*\*\*TABLE 3 NEAR HERE\*\*\***

249

250 **Discussion**

251 The purpose of this study was to determine if analysis of the accelerometry data can provide  
252 actionable insight into training induced disruptions with no further testing on the athlete. This  
253 study has presented novel data showing that variability in stride detected by commonly used

254 accelerometers is associated with fatigue, soreness and training load. The ability to identify times  
255 when an athlete is at risk of injury or requires a training modification to maximize their  
256 performance in subsequent activities (whether that be a reduction or increase to their training load)  
257 is crucial in the preparation of athletes for competition.

258

### 259 *Load & Wellness*

260 The more fatigued athletes reported being the lower their stride variability. Previously with  
261 fatigue it has been shown that along with increased leg stiffness, the vertical motion of the CoM  
262 significantly reduces with prolonged exhaustive running.<sup>16</sup> However, few studies have previously  
263 used trunk accelerometry to assess running related fatigue.<sup>17-19</sup> In contrast to the current study,  
264 one study found a decrease in regularity of vertical CoM accelerations, when sub-elite distance  
265 runners underwent a short but highly intensive track run to exhaustion.<sup>19</sup> Similarly, another  
266 showed that treadmill running-induced fatigue results in anteroposterior trunk accelerations that  
267 are less regular from step-to-step and are less predictable.<sup>18</sup> The final study showed that CoM  
268 movement could accurately estimate increases in metabolic work during an incremental running  
269 protocol to exhaustion.<sup>17</sup> It may be that the increased variability seen with these American Football  
270 players may signal a re-organization of motor strategies for the purpose of preserving performance  
271 (i.e. this increased stride variability may manifest as decreased variability in the upper body).

272

273 Previous research has demonstrated that fatigue alters the way player load is accumulated in  
274 Australian Rules Football matches.<sup>20</sup> Other authors found that a one unit decrease in wellness Z-  
275 score resulted in a 4.9% (standard error 3.1%) and 8.6% (standard error 3.9%) decrease in player  
276 load and player load slow (running activity < 2 m.s<sup>-1</sup>), respectively.<sup>21</sup> Players with reduced  
277 wellness may maintain the running variables that they deem critical to performance but modify  
278 other aspects of activity profile such as change of speed, low speed running and/or body contact  
279 that were not measured in this study.<sup>22</sup>

280

281 Within American Football specifically it has been shown that a one unit increase in wellness z-  
282 score and energy were associated with a trivial 2.3% and 2.6% increase in player load.<sup>12</sup> A one  
283 unit increase in muscle soreness (players felt less sore) corresponded to a trivial 4.4% decrease in  
284 s-RPE training load. In addition, significant ( $p < 0.05$ ) differences in movement variables were  
285 demonstrated for individuals who responded more or less favorably on their rating of perceived  
286 wellness.<sup>23</sup> In the current study while, there were no associations with sleep a decreased soreness  
287 resulted in an increase in variability – further investigations may look at the relationship between  
288 variability and sRPE directly.

289

290 An increase in load (both acute (7d) and chronic (21d) saw an increased variability in these team  
291 sport athletes. Although the mechanism underlying this increase in variability is currently unclear,  
292 it is roughly in agreement with previous theories<sup>2,24</sup>, that suggest that a shift away from an  
293 individual's optimal level of variability is indicative of a pathological state. A shift to an increased  
294 level of variability could be a sign of a noisy and irregular system, which has been demonstrated  
295 to be a characteristic of individuals who had undergone knee reconstructions to repair a damaged  
296 anterior cruciate ligament<sup>25</sup> (possibly due to not being able to restore the proprioceptive pathways  
297 found in a healthy knee).

298

299 There is a high practical value to these findings as while current metrics do have the ability to  
300 predict injury risk, especially when examining cumulative load measures,<sup>26</sup> they require a full  
301 training history to identify periods of load, (be that acute or chronic in nature), whereas if there is  
302 data missing or unavailable (such as when athletes are recruited into a squad on an intermittent  
303 basis or miss days through modified training) then the methods outlined here will still be able to  
304 identify individual athletes who have an elevated period of load compared to their normal training  
305 load (provided a baseline level of healthy movement variability has already been established).

306

307 *Compromised Training*

308 While there was an increased odds ratio of decreased variability in the presence of a flagged  
309 hamstring the analysis was too underpowered to draw a conclusion. Reduced variability would be  
310 expected for an acute injury. It has been observed that ACL deficient patients<sup>25</sup> have less step-to-  
311 step variability in walking gait, inferring that they are being more “careful” when they were  
312 walking, trying to eliminate extraneous movements. The authors speculate that participants may  
313 be attempting to constrain movements and reduce step-to-step variability within the current  
314 results. The hamstring conditions likely indicate a compromised system. Further study may reveal  
315 if these flags are more indicative of chronic rather than acute conditions and so athletes have  
316 developed strategies to cope in these circumstances.

317

318 **Limitations**

319 The current investigation was limited to a single team over a single season, but still includes a  
320 total of 127,715 strides collected across 1177 sessions and 443 matches. A wider group would  
321 allow comparisons of differing training styles and approaches. Analyzing the occurrence of self-  
322 reported flags set at an arbitrary level (5/10) can be criticized as not everyone views discomfort in  
323 the same way and so potentially looking at an individual comparison may improve this metric.

324

325 Also, there were limited flags compared to the number of injuries that occur in collegiate football.  
326 The typical injury rates would suggest that 20% of injuries are in the knee<sup>27</sup> but these may be  
327 catastrophic one-off issues (i.e. ACL) rather than a degenerative issue that can be detected by  
328 flagging in a routine questionnaire. So, while early detection of issues as this study has shown  
329 possible is key, the differing positional demands and subsequent injury rates may need future  
330 studies to delineate the effects for particular positions in American Football in the context of injury  
331 history.

332

333 *Practical Applications*

334 The difference in the measures outlined is that predictions can be made from physical symptoms,  
335 but these track well with at least some of the subjective markers that athletes are giving. What is  
336 not known is how many athletes are not accurately flagging symptoms of soreness and so are  
337 going undetected in this analysis. In the absence of 100% disclosure from athletes the assessment  
338 of variability therefore has the potential to identify athletes who are displaying physical symptoms  
339 that would indicate the need to modify training. Conversely, it may be able to identify athletes  
340 who do satisfy flagging criteria but are showing no physical symptoms who therefore may not  
341 need training modifications.

342

343 *Conclusions*

344 This study has shown that stride variability is associated with fatigue and 7-day training load.  
345 Combining both objective and subjective methods is likely to enhance the predictive ability and  
346 become a very powerful tool within elite sport environments, and while further investigations into  
347 this are warranted, the assessment of variability has the potential to identify athletes who are  
348 displaying physical symptoms that would indicate the need to modify training.

349 **References**

- 350 1 Bartlett R, Wheat J, Robins M. Is movement variability important for sports  
351 biomechanists? *Sport Biomech* 2007; 6(2):224–243. Doi: 10.1080/14763140701322994.
- 352 2 Hamill J, Palmer C, Van Emmerik RE. Coordinative variability and overuse injury. *Sports*  
353 *Med Arthrosc Rehabil Ther Technol* 2012; 4(1):45. Doi: 10.1186/1758-2555-4-45.
- 354 3 Heiderscheit BC, Hamill J, Van Emmerik RE. Variability of stride characteristics and joint  
355 coordination among individuals with unilateral patellofemoral pain. *J Appl Biomech* 2002;  
356 18(2):110–121. Doi: 10.1123/jab.18.2.110.
- 357 4 Cortes N, Onate J, Morrison S. Differential effects of fatigue on movement variability.  
358 *Gait Posture* 2014; 39(3):888–893. Doi: 10.1016/j.gaitpost.2013.11.020.
- 359 5 Wundersitz DWT, Gastin PB, Richter C, et al. Validity of a trunk-mounted accelerometer  
360 to assess peak accelerations during walking, jogging and running. *Eur J Sport Sci* 2015;  
361 15(5):382–390. Doi: 10.1080/17461391.2014.955131.
- 362 6 Buchheit M, Gray A, Morin JB. Assessing stride variables and vertical stiffness with GPS-  
363 embedded accelerometers: Preliminary insights for the monitoring of neuromuscular  
364 fatigue on the field. *J Sport Sci Med* 2015; 14(4):698–701. Doi:  
365 10.1519/JSC.0000000000001017.
- 366 7 Farana R, Jandacka D, Uchtyl J, et al. the Effect of Different Hand Position on Impact  
367 Forces and Elbow Loading During the Round Off in Female Gymnastics. *31 Int Conf*  
368 *Biomech Sport* 2013; 5(2):5–14.
- 369 8 Buckeridge E, LeVangie MC, Stetter B, et al. An on-ice measurement approach to analyse  
370 the biomechanics of ice hockey skating. *PLoS One* 2015; 10(5). Doi:  
371 10.1371/journal.pone.0127324.
- 372 9 Buttfield A. *The Development and Application of a Novel Method of Analysing Within-*  
373 *step Accelerations Collected During Australian Rules Football Games*. Victoria  
374 University, 2016.
- 375 10 Casals M, Finch CF, FlowingData, et al. Sports Biostatistician: a critical member of all



- 376 sports science and medicine teams for injury prevention. *Inj Prev* 2016; 14(20):e1002430.  
377 Doi: 10.1136/injuryprev-2016-042211.
- 378 11 Wellman AD, Coad SC, Flynn PJ, et al. A Comparison of Pre-Season and In-Season  
379 Practice and Game Loads in NCAA Division I Football Players. *J Strength Cond Res*  
380 2017; (201):1. Doi: 10.1519/JSC.0000000000002173.
- 381 12 Govus AD, Coutts A, Duffield R, et al. Relationship Between Pretraining Subjective  
382 Wellness Measures, Player Load, and Rating-of-Perceived-Exertion Training Load in  
383 American College Football. *Int J Sports Physiol Perform* 2018; 13(1):95–101. Doi:  
384 10.1123/ijsp.2016-0714.
- 385 13 Neville JG, Rowlands DD, Lee JB, et al. A Model for Comparing Over-Ground Running  
386 Speed and Accelerometer Derived Step Rate in Elite Level Athletes. *IEEE Sens J* 2016;  
387 16(1):185–191. Doi: 10.1109/JSEN.2015.2477497.
- 388 14 Kadaba MP, Ramakrishnan HK, Wootten ME, et al. Repeatability of kinematic, kinetic,  
389 and electromyographic data in normal adult gait. *J Orthop Res* 1989; 7(6):849–860. Doi:  
390 10.1002/jor.1100070611.
- 391 15 Sampson JA, Murray A, Williams S, et al. Injury risk-workload associations in NCAA  
392 American college football. *J Sci Med Sport* 2018. Doi: 10.1016/j.jsams.2018.05.019.
- 393 16 Morin J-B, Samozino P, Millet GY. Changes in running kinematics, kinetics, and spring-  
394 mass behavior over a 24-h run. *Med Sci Sports Exerc* 2011; 43(5):829–836. Doi:  
395 10.1249/MSS.0b013e3181fec518.
- 396 17 Mcgregor SSJ, Busa MMA, Yaggie JA, et al. High Resolution MEMS Accelerometers to  
397 Estimate VO<sub>2</sub> and Compare Running Mechanics between Highly Trained Inter-Collegiate  
398 and Untrained Runners. *PLoS One* 2009; 4(10):1–10. Doi: 10.1371/journal.pone.0007355.
- 399 18 Schütte K, Maas EA, Exadaktylos V, et al. Wireless Tri-Axial Trunk Accelerometry  
400 Detects Deviations in Dynamic Center of Mass Motion Due to Running-Induced Fatigue  
401 2015:1–12. Doi: 10.1371/journal.pone.0141957.
- 402 19 Le Bris R, Billat V, Auvinet B, et al. Effect of fatigue on stride pattern continuously  
403 measured by an accelerometric gait recorder in middle distance runners. *J Sports Med*

- 404 *Phys Fitness* 2006; 46(2):227–231.
- 405 20 Cormack S, Mooney MG, Morgan W, et al. Influence of neuromuscular fatigue on  
406 accelerometer load in elite Australian football players. *Int J Sports Physiol Perform* 2013;  
407 8(4):373–378. Doi: 10.1123/ijsp.8.4.373.
- 408 21 Gallo TF, Cormack S, Gabbett TJ, et al. Pre-training perceived wellness impacts training  
409 output in Australian football players. *J Sports Sci* 2015; 0414(December):1–7. Doi:  
410 10.1080/02640414.2015.1119295.
- 411 22 Coutts AJ, Quinn J, Hocking J, et al. Match running performance in elite Australian Rules  
412 Football. *J Sci Med Sport* 2010; 13(5):543–548. Doi: 10.1016/j.jsams.2009.09.004.
- 413 23 Wellman AD, Coad SC, Flynn PJ, et al. Movement Demands and Perceived Wellness  
414 Associated With Preseason Training Camp in NCAA Division I College Football Players.  
415 *J Strength Cond Res* 2017; 31(10):2704–2718. Doi: 10.1519/JSC.0000000000002106.
- 416 24 Stergiou N, Harbourne RT, Cavanaugh JT. Optimal Movement Variability: A New  
417 Theoretical Perspective for Neurologic Physical Therapy. *J Neurol Phys Ther* 2006;  
418 30(3):120–129. Doi: 10.1097/01.NPT.0000281949.48193.d9.
- 419 25 Stergiou N, Decker LM. Human movement variability, nonlinear dynamics, and  
420 pathology: Is there a connection? *Hum Mov Sci* 2011; 30(5):869–888. Doi:  
421 10.1016/j.humov.2011.06.002.
- 422 26 Colby MJ, Dawson B, Heasman J, et al. Accelerometer and GPS-derived running loads  
423 and injury risk in elite Australian footballers. *J Strength Cond Res* 2014; 28(8):2244–2252.  
424 Doi: 10.1519/JSC.0000000000000362.
- 425 27 Krill MK, Borchers JR, Hoffman JT, et al. Analysis of Football Injuries by Position Group  
426 in Division I College Football : A 5-Year Program Review. *Clin J Sport Med* 2018; 0(0).
- 427
- 428

429

430 **Figure Captions**

431 **Figure 1:** Within- and Between-stride CMD over the season for individuals, with group  
432 mean in bold

433 **Figure 2:** Standardized (z-scored) effects of wellness and load on CMD

434 **Table Captions**

435 **Table 1:** Descriptive statistics for the 63 American Football athletes

436 **Table 2:** Linear Mixed Model Outputs

437 **Table 3:** Results from a generalized linear mixed model of flagged events